

# EROSION ON GLASS IONOMER CEMENT AND THEIR ADDITION: A REVIEW

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## Abstract

**Introduction:** Glass ionomer cement (GIC) is a type of tooth-coloured dental restorative material that is commonly used nowadays. This restorative material is commonly exposed to an intrinsic and extrinsic erosive oral environment which affects the integrity of the restoration. All along, many modifications have been done to improve the properties of conventional GIC (cGIC) while maintaining its clinical advantages. Several studies have been conducted to compare the effects of erosion on cGIC and their modification. **Objectives:** This literature review aims to analyze the effect of erosion on cGIC, RMGIC, and its modifications. **Methods:** A literature search was performed using PubMed, Scopus, and Web of Science databases to identify the related articles that are within the research interest using multiple keyword combinations. Searches were limited to articles that were published from the year 1990 to 2019. Seventy-four articles that fit the research criteria were selected. **Results:** Conventional GIC had been greatly affected when exposed to low pH solutions such as hydrochloric, phosphoric, and citric acid. It showed greater mean of surface microhardness loss, solubility, and microleakage compared to RMGIC that was modified with resin addition. The modification with casein phosphopeptide-amorphous calcium phosphate (CPP-ACP) showed no changes in surface microhardness loss when exposed to an acidic medium. **Conclusion:** Conventional GIC is more affected in an acidic environment compared to after its modification such as RMGIC and CPP-ACP modified cGIC. Patients with high risk exposure to erosive environment should not be restored only by cGIC unless it is used in closed-sandwich technique restoration.

**Keywords:** acid challenges on dental materials, erosion on GIC modifications, GIC erosion, pH effect on GIC and its modifications, RMGIC erosion effect.

## Main text

### Introduction

Glass ionomer cement is a type of tooth-coloured dental restorative material which were invented in 1969 and reported by Wilson and Kent in the early 1970s [1,2]. Conventional GIC (cGIC) is mainly composed of three essential ingredients, namely polymeric water-soluble acid (polyalkenoic acid), ion-leachable glass (calcium aluminofluoro-silicate glass powder), and water [3,4]. The components in cGIC undergo an initial setting within 2 to 6 minutes through acid-base reaction [5]. The maturation process of the cement takes place after 24 hours of initial setting, so the cement should be prevented from dehydration by the placement of surface protection coatings such as petroleum jelly [5,6,7].

Physical properties of cGIC include the ability to form a chemical bond with tooth enamel and dentine through an ion exchange mechanism, able to release fluoride and act as fluoride reservoir by absorbing salivary fluoride from dentifrices, mouthwashes and topical fluorides as well as possesses similar coefficient of thermal expansion as dentine [1,8,9]. These properties make it suitable to be used as temporary restoration, atraumatic restorative treatment (ART) material, cavity liner/base, fissure sealant and luting cement [10]. However, cGIC exhibits low fracture toughness, wear resistance and mechanical strength which limits their usage at high stress-bearing areas [1,8]. Conventional GIC also exhibits an initial slow setting which in turn makes it sensitive to moisture, low early strength as well as progressive loss of cGIC which will eventually cause the failure of the restoration [11]. To overcome these drawbacks, many modifications have been done on cGIC such as resin-modified glass ionomer cement (RMGIC), bioactive glass reinforced glass ionomer cement, silica-reinforced glass ionomer cement, zinc-based glass ionomer cement, GIC-nanohydroxyapatite-silica-zirconia, casein phosphopeptide-amorphous calcium phosphate (CPP-ACP) and many more [2,12]. The most widely used modified GIC is RMGIC which was introduced in the early 1990s [13]. Resin modified GIC is a hybrid of cGIC

and light-curing resin which sets by photo-polymerization[1,13]. The properties of RMGIC were found to have less moisture sensitivity, early cement strength, improved physical and mechanical properties, and better bond strength to the tooth structure as compared to cGIC[1,14].

Dental erosion is the progressive loss of dental hard tissues caused by a chemical process and does not involve bacterial action[14,15]. In current days, high consumption of acidic drinks and beverages due to easier to get can cause restorative materials commonly exposed to the effect of erosion by causing tooth sensitivity, toothache and severe wear. An intrinsic erosive environment includes gastric acid reflux or excessive vomiting while an extrinsic environment includes carbonated drinks or medications. Thus, it is important to know the ability of the dental restorative materials to withstand erosion. Various techniques can be applied to evaluate the loss of dental materials after erosive exposure. The most frequently used techniques are scanning electron microscope (SEM), profilometry, stereomicroscope, microradiography, and iodide permeability test[16]. Hence, this review will be done on literature related to erosion on GIC and its modification which might be able to help operators selecting better options for patient's treatment when there is an acidic mouth environment.

### **Methodology**

#### ***Search strategy and study selection***

A literature search was performed using electronic databases such as PubMed, Scopus, and Web of Science to identify the related articles that are within the research interest. The inclusion criteria for this review are articles that were published from the year 1990 to 2019 with different combinations of the following keywords: "GIC erosion", "pH effect on GIC and its modifications", "acid challenges on dental materials", "RMGIC erosion effect" and "erosion on GIC modifications". The exclusion criteria are articles that were written in a foreign language and have no abstracts available. Articles that fulfilled the criteria for this study were selected, the information was assessed, gathered and a report was written.

### **Results**

Seventy-four articles that follows the criteria were selected which comprise of 30 articles from PubMed, 24 from Scopus and 20 from Web of Science as tabulated in Table 1.

#### ***Technique of assessing erosion effect on GIC***

From the literature review search, few techniques had been used by researchers in assessing the erosion effect on dental materials, specifically GIC [17]. This includes scanning electron microscope (SEM), profilometer, and stereomicroscope. The SEM is one of the most frequently used devices for assessing erosion due to easily used and availability especially for descriptive assessment as it produces three-dimensional representation that is useful for understanding the surface structure of the sample[17]. The second most common technique used is the profilometer where the technique uses probe tip movement to assess the surface roughness of eroded specimens as it has sufficient sensitivity to investigate early tooth tissue loss produced by limited exposure to acid[18,19]. Some researchers use stereomicroscope due to its simplicity in measuring the depth of erosion or use code for grading [16]. A clinical photograph is not popularly used because the photographs may not give an accurate result of the extent of erosion and the quality of the outcome depends on the photographer's dexterity and light reflectivity[17]. Other techniques such as polarized light microscopy, Dynamic Secondary Ion Mass Spectrometry (DSIMS), Non-Contact Confocal Laser Scanning Microscopy, Scanning Acoustic Microscope (SAM), and etc. had been used but no so popular [17].

#### ***Effects of different erosive solutions on GIC and its modifications.***

Several studies have been conducted to investigate the effect of erosion on tooth-coloured dental restorative materials especially GIC. Generally, cGIC was significantly degraded with erosion. Different erosive solutions or drinks showed a different level of degradation to GIC and its modification. The effect may be or may not be related to the pH but the type of acid usually plays a role. In one study, both cGIC and RMGIC were significantly eroded by five different acidic drinks but not all in proportionate with the pH of the acidic drinks [20]. Coke® and orange juices show greater erosive effect and pineapple juice caused the least erosion for both cGIC and RMGIC. Different result seen in another study by Aliping-McKenzie *et al.* (2004) where the tooth-coloured dental restorative materials were severely eroded in fruit juices but lesser when compared to Coke[21]. Orange juice containing citric acid and apple juice containing maleic acid showed greater erosive threat compared to Coke that contains phosphoric acid.

The erosion effect also shows different features in different areas where erosion at the body might be different from the margin of restoration. A study found that Coke® with lower pH (pH 2.58) showed greater erosion at the body of restoration whereas marginal erosion depth was greater in orange juices (pH 3.41) [20]. The study also found that margins of the cGIC restoration had greater dissolution compared to the body of the restoration especially when immersed in citric acid solution. Different types of materials being affected differently by erosion. Resin-modified GIC showed only minimal damage when compared to cGIC while composite resin (CR) and porcelain have no changes[22]. Thus, the authors stated that cGIC is not suitable for patients having strong citric acid or gastric acid-induced erosion but closed sandwich restorations may be performed [22]. Different combinations of acids also give different erosive results such as Coke containing

carbonic and phosphoric acid (pH 2.5) has a greater effect on the surface microhardness of cGIC compared to another Coke containing carbonic and citric acid (pH 2.98) [23].

A study was done for the Malaysian population concerning few popularly consumed tropical juices by assessing at the surface roughness of the CR, cGIC, and RMGIC which found that tamarind juice (pH 3.00) had the greatest erosive effect on the materials compared to mango juice (pH 3.11) and pineapple juice (pH 3.18) after being immersed for a day [24]. Minimal change in pH gives the differences. Another study's finding was orange juice (pH 2.85) greatly affects the surface roughness and solubility of cGIC [25]. In this study, the cGIC was severely eroded by hydrochloric and citric acid solutions while minimally eroded by phosphoric acid following two hours of exposure. Another study showed an identical result whereby the newer and the older generation of GIC which are GC Fuji® VII, GC Fuji® Bulk, GC Fuji® IX Fast, Fuji® IX Extra, and GC Equia® Forte Fil completely dissolved in citric acid (pH 3.5-4.0) after 7 days followed by phosphoric acid (pH 2-3) and lactic acid (pH 4-4.5) [26]. Assessment on the erosion in post-radiation xerostomic patients revealed that cGIC had the greatest failure related to the marginal adaptation and anatomical form after 24 months regardless of the use of neutral pH sodium fluoride gel compared to RMGIC and composite resin [27]. This result is similar to a study conducted by Viana *et al.* in 2020 [28]. Conventional GIC had significantly higher surface loss values compared to RMGIC, CR, and compomer which shows a similar result as a study done by Babita *et al.* whereby GIC shows the highest value for the mean of change in average surface roughness when immersed in Coke (pH 1.87) compared to CR and compomer [18,29].

Scarce of studies were found on the erosion of modified GIC else than RMGIC. Casein phosphopeptide-amorphous calcium phosphate (CPP-ACP) modified GIC were found to have the ability to release fluoride, calcium, and phosphate ions under acidic solutions compared to cGIC that only releases fluoride in response to an acidic environment [30]. The CPP-ACP acts to repair by remineralizing the acid-eroded enamel surface to produce a higher nanoindentation hardness of the remineralized enamel [31]. However, a study found that the CPP-ACP modified GIC is ineffective in preventing erosive effect and remineralization of enamel that subjected to extrinsic erosion [32,33].

## Discussion

### *Classification of GIC*

Glass ionomer cement can be classified based on its clinical use into Type I, Type II, and Type III [11]. The type of GIC used is important as it influences the outcome of clinical procedure and the satisfaction of the patient. Type I GIC is a radiopaque cement that is used as luting and bonding in cementation of crowns, bridges, inlays, onlays, and orthodontic bands [1,11]. This type of cement has moderate strength with a relatively low powder:liquid ratio (1.5:1 to 3.8:1). Besides, it has fast-setting properties that provide an early resistance to water [11]. Type II GIC is used as restorative cement and could be further divided into 2 types depending on the importance of the appearance. Type II GIC (1) is used for anterior repairs whereby the aesthetics are the priority as it has a good colour match and translucency [11,13]. This type of GIC is usually radiopaque and has a high powder:liquid ratio (3:1 to 6.8:1). However, this type of GIC needs protection from moisture for at least 24 hours with petroleum jelly or varnish [11,13]. Type II GIC (2) is usually radiopaque and being used for posterior restorations or repairs whereby the aesthetics are not the priority [11,13]. This type of GIC has a high powder:liquid ratio (3:1 to 4:1) with fast setting properties that make it having early resistance to water uptake [11]. Type III GIC is a radiopaque cement used as a lining or base cement. For liners, the powder:liquid ratio is low (1.5:1) to allow good adaptation of the cement to the cavity walls. For bases, the powder:liquid ratio is high (3:1 to 6.8:1) as the base acts as dentine replacement [11,13]. Due to many weaknesses, the cGIC had been modified by the addition of a few materials or powder.

### *Methods of assessing erosion on dental materials especially GIC*

Several techniques could be used to evaluate the effect of erosion on the dental materials. For *in-vitro* techniques, Scanning Electron Microscope (SEM) was one of the first techniques to determine the *in-vitro* resorption of dental hard tissues [34]. It reveals the effects of superficially deposited precipitates resulted from mineral dissolution by various agents [35,36]. It can also evaluate the efficacy of salivary pellicle and dental plaque in protecting underlying the enamel surfaces from acidic dissolution [34,35]. Besides, SEM readings are highly reproducible and can be performed on both polished and unpolished native surfaces after gold-sputtering, which mimics conditions at the tooth surface [17].

Surface profilometry is also an *in-vitro* technique that quantifies the dental tissue loss using non-treated area as a reference [35]. It also gives information on the surface roughness where the surface of the sample can be scanned to produce a 2D or 3D profile using a contact or non-contact measuring device [39]. Erosive lesions with 0.5  $\mu\text{m}$  depth can be constantly detected and also measured using non-contact profilometry [40]. Stereomicroscope is another device which is used to measure the depth of erosion and a 3-dimensional images can be produced for better view of the sample [34]. The data for measurement depth of erosion could be tabulated in micrometer or using code as classification [22]. Polarized light microscopy is another *in-vitro* technique used to measure the depth of lesion by observing the crystal birefringence changes in cross-sections of

dental erosion specimens[41]. This technique can be used to observe organic and inorganic rigid and repeatable structures. For eroded dentine, this technique discriminates between the partly or fully demineralized tissues in the form of the pore volume.

Non-Contact Confocal Laser Scanning Microscopy (CLSM) is an *in-vitro* technique that produces high-resolution 3D optical images with depth selectivity from sample[17]. This technique does not require sample preparation while visualizing the surfaces[17]. It has high resolution and fast recording of surface topography and can be used for quantifying erosive tissue loss and softening depth[42]. Scanning Acoustic Microscope (SAM) is another *in-vitro* technique that can be used for the evaluation of local physico-mechanical properties of tooth microstructure[43]. This technique has more advantages if compared to other conventional devices as it does not require any preparation for tooth tissue study as it uses focused sound to investigate, measure or produce the image of an object[44]. This is a sensitive technique, however, is less specific as it could not differentiate between erosion, abrasion, and abfraction[44]. Besides, Dynamic Secondary Ion Mass Spectrometry (DSIMS) allows semi-quantitative analysis of the elemental and molecular composition of specimen surfaces[16]. Secondary ion mass spectroscopy studies the enamel erosion and fluoride uptake by early erosive lesions[45]. This technique has excellent sensitivity and allows the visualization of 2D and 3D images[46].

Clinical examination and use of photographs is an *in-vivo* technique used in measuring the enamel defect and dental erosion by taking radiographs[17]. Clinical photographs are very useful in monitoring erosive wear in patients[47] and they have the potential in comparing erosion measurements[48]. Quantitative Light-Induced Fluorescence (QLF) is an *in-vitro/in-vivo* technique based upon the auto-fluorescence of enamel whereby the decrease in mineral content will decrease its fluorescence[17]. This technique could be used to detect any early mineral changes in enamel and can be used for longitudinal assessment[49]. The demineralized areas will appear darker which could help in measuring the amount of erosion[50]. However, this technique is expensive and could cause problematic probe positioning[17]. Optical Coherence Tomography (OCT) is a high-resolution and non-invasive technique that assesses the degree of mineral loss in enamel[35]. This technique is limited to *in-vivo* accessibility and the presence of enamel erosion will result in a change in optical properties[51]. Atomic Absorption Spectrophotometry (AAS) is an *in-vitro/in-vivo* technique that uses optical light absorption to quantify the erosion on enamel and dentine[17]. They are expensive but the measurements are possible and non-destructive longitudinal. It has been used to check the enamel dissolution by measuring the calcium in acid etch solutions[52].

A digital pH meter is used to determine the pH of food and drinks by measuring the number of hydrogen ions. The pH of beverages is considered acidic if the pH value is low which shows there is a high concentration of hydrogen ions[17]. It was also used to measure salivary pH before and after consumption of soft drink or the pH of beverages with erosive potential [53]. Another technique for assessing erosion is by microindentation and nanoindentation technique which assess the surface hardness by measuring the resistance of a substance to indentation[17]. Microindentation is measured using Knoop or Vicker's diamond indenter while nanoindentation is measured using Berkovich diamond indenter. Both microindentation and nanoindentation techniques require less cost and are less destructive. These techniques may be inaccurate in measuring the erosion at highly eroded areas. Ultrasonication and chemical analysis is a non-destructive technique that can be used for the early diagnosis of dental erosion and longitudinal measurement of progressive enamel loss[54]. This technique however could cause poor probe positioning and poor reliability in the measurement of enamel thickness changes of less than 300µm[55].

In general, many techniques were available in evaluating the erosion effect; whereby each technique has its advantages and disadvantages[17]. It shows that *in-vivo* technique achieve greater sensitivity, specificity, and accuracy in measuring tooth loss compared to *in-vitro* technique which mainly could mimic an oral conditions[34].

#### **Addition for modifications of cGIC**

Conventional GIC has few weaknesses in physical and mechanical properties. Due to many weaknesses, various types of phase reinforcements and modifications with the addition of materials or powders were done for GIC composition by researchers to improve its properties. Nano-silver modified GIC has been synthesized to impart antibacterial activity and improving mechanical properties [56]. This modification has been reported to have an improved handling characteristic, increased compressive strength, and significant antimicrobial activity with increasing concentration of the nano-silver particles [56]. Nano titanium oxide-modified GIC showed an increase in compressive strength and flexural strength compared to cGIC[57]. Reinforcement of bioactive glass powder (BAG) to cGIC showed a stable bond to the tooth through the peptide layer and had antimicrobial properties depending on the composition of the BAG[58]. Another study was done on BAG-GIC hybrid by mixing 10% or 30% of BAG particles with cGIC and RMGIC. The compressive strength of the BAG-GIC hybrid decreased with the increasing amount of BAG[59]. This study also showed that the cGIC-BAG material on average had 55% higher surface microhardness compared to RMGIC-BAG.

Another modification of GIC includes reactive glass fiber reinforced glass ionomer cement. A study was conducted to evaluate the fracture toughness and total amount of energy released from this enhanced GIC[60]. There was an increase in fracture toughness of 140% and the total amount of energy released was 440% compared to cGIC. Another similar study reported that the reinforcement of the hollow and solid discontinuous fiber fillers with 2 different loading fractions resulted in increased fracture toughness and flexural strength of cGIC and RMGIC[61]. Glass ionomer cement was also reinforced by hydroxyapatite to enhance the mechanical properties. A study was conducted on this hybrid showed that the addition of nano-hydroxyapatite and fluorapatite into cement resulted in higher compressive strength, diametral tensile strength, and biaxial flexural strength compared to the cGIC[62]. The bonding of the tooth-ionomer interface has been enhanced by decreasing the size of apatite from micrometer to nanometre scale[63]. In another study, cGIC has been reinforced with hydroxyapatite and silica nanocomposite which showed an increase in the hardness[64]. This silica reinforced glass ionomer was synthesized in an attempt to improve cGIC translucency and increase the number of polysalt bridges in the glass matrix. The hardness, compressive strength, and flexural strength of 35%  $SiO_2$  is higher compared to 11% and 21% of  $SiO_2$ [64].

Zinc-based glass ionomer cement contains zinc oxide which can act as network modifying oxide and an intermediate oxide[65]. A lower concentration of Ca increases the susceptibility of the glass to attack which causes it to be more bioactive[66]. A study using niobium pentoxide that was incorporated into GIC to enhance the mechanical properties and exhibits good biocompatibility and bioactivity[67]. It showed that the setting time of the cement increased with the increasing amount of Nb in GIC but the mechanical properties are adversely affected[65]. Another recent modification, cGIC has been reinforced with hydroxyapatite, silica and zirconia nanocomposite under a controlled grinding process and it showed an increase in the hardness, Young's modulus, and bioactivity compared to cGIC[68]. This GIC-nano-hydroxyapatite-silica-zirconia has shown significant improvement in mechanical, physical, chemical and biological properties. The hardness increased with an increase in the nano-zirconia content up to 5%. This makes it possible to be used for wider scope such as higher stress bearing area, for restoration of permanent dentition and stronger ART material [67,68]. Casein Phosphopeptide-Amorphous Calcium Phosphate (CPP-ACP) has been shown to promote the remineralization of enamel as well as prevents demineralization [69,70].

#### ***Erosion effect of GIC and its modification***

Not many studies were found in the literature for the erosion of GIC and its modification. The erosion of dental materials was found to be influenced by the hydrogen ion concentration, titratable acidity, acid strength, buffering capacity and chelating function of the acid [18,24]. The amount of the actual hydrogen ions (titratable acid) significantly influence the erosive effect on dental materials [20,21]. Low pH beverages could adversely affect the properties of the tooth-coloured dental restorative materials [25]. As the pH of the solutions decreased, the hardness of the material decreases while the surface roughness and the solubility of the material increase [25]. The frequency of immersion significantly affects the surface roughness of RMGIC due to the replacement of the hydrogen ion in the GIC with the metal cations in the matrix which will eventually cause more dissolution [71].

Many studies accept that pH is an important factor that contributes to the erosion effects of tooth-coloured dental restorative materials but many other studies suggest that the composition is more important factor [21,71]. In a case where citric acid has a higher pH value compared to phosphoric acid, citric acid has a greater effect on cGIC as it has a larger equilibrium constant which allows increased protons exchange for the dissolution of GIC in its solution [26]. Also, the presence of phosphoric acid suppresses the dissolution rate of calcium and phosphate from the tooth [72]. Thus, the composition of the fruit juices has a greater influence on the dental restorative materials compared to the pH of a drink [21,73].

Many other factors influence the roughness of the material such as the shape difference, distribution, number of particles, and the interfacial bonding between particles and matrix [29]. Conventional GIC having more erosion compared to RMGIC which might be due to the formation of a leachable layer that can inhibit degradation of the material and ability to reduce the acidity of the acidic solutions [74]. The presence of resin would reduce the acid challenge intensity making RMGIC have lower susceptibility to erosion compared to cGIC[28,69,70,71]. Hence, beverages containing lower pH has more erosive effect but the type, concentration, acid amount, calcium chelating properties, exposure time and temperature, and buffering capacity of the saliva also affects the dissolution in the oral cavity [18].

#### **Conclusion**

From this review, it was shown that cGIC is more affected in an acidic environment compared to RMGIC and other modified cGICs. Erosive environment affects cGIC physical properties whereby its surface microhardness loss, solubility, and microleakage is greater than RMGIC and CPP-ACP modified cGIC. Therefore, patients with a high risk of being exposed to an erosive environment should avoid cGIC restoration to maintain the integrity of the restoration and quality of life unless cGIC is used in closed-sandwich technique restoration.

**8.0 References:**

1. Croll TP, Nicholson JW. Glass ionomer cements in pediatric dentistry : review of the literature. *Pediatr Dent*2002;24 Suppl 5:423–9.
2. Moheet IA, Luddin N, Rahman IA, Kannan TP, Nik Abd Ghani NR, Masudi SM. Modifications of glass ionomer cement powder by addition of recently fabricated nano-fillers and their effect on the properties: A Review. *Eur J Dent* 2019;13 Suppl 3:470–7.
3. Wilson AD. Glass-ionomer cement origins, development and future. *Clin Mater* 1991;7 Suppl 4:275–82.
4. McLean JW, Nicholson JW, Wilson AD. Proposed nomenclature for glass-ionomer dental cements and related materials. *Quintessence Int* 1994;25 Suppl 9:587–9.
5. Nicholson JW. Maturation processes in glass-ionomer dental cements. *Acta Biomater Odontol Scand* 2018;4 Suppl 1:63–71.
6. Lohbauer U. Dental glass ionomer cements as permanent filling materials? -Properties, limitations and future trends. *Mater (Basel)* 2010;3 Suppl 1:76–96.
7. Kamatham R, Reddy S. Surface coatings on glass ionomer restorations in Pediatric dentistry-Worthy or not. *J Indian Soc Pedod Prev Dent* 2013;31 Suppl 4:229–33.
8. Forsten L. Fluoride release and uptake by glass-ionomers and related materials and its clinical effect. *Biomater* 1998;19 Suppl 6:503–8.
9. Sidhu S, Nicholson J. A review of glass-ionomer cements for clinical dentistry. *J Funct Biomater* 2016;7 Suppl 3:16.
10. Khairiyah Abd Muttalib. Guidelines on the use of glass ionomer cements. Ministry of Health Malaysia;2014.
11. Kim Y, Hirano S and Hirasawa T. Physical properties of resin-modified glass-ionomers. *Dent Mater* J1998;17 Suppl 1:68–76.
12. Sajjad A, Wan Bakar W, Mohamad D, Kannan T. Various recent reinforcement phase incorporations and modifications in glass ionomer powder compositions: A comprehensive review. *J Int Oral Heal* 2018;10 Suppl 4:161–7.
13. Sidhu SK, Watson TF. Resin-modified glass ionomer materials. A status report for the American Journal of Dentistry. *Am J Dent* 1995;8 Suppl 1:59-67.
14. Shaw L, Smith AJ. Dental erosion - The problem and some practical solutions. *Br Dent J* 1999;186 Suppl 3:115–8.
15. Wongkhantee S, Patanapiradej V, Maneenut C, Tantbirojn D. Effect of acidic food and drinks on surface hardness of enamel, dentine, and tooth-coloured filling materials. *J Dent* 2006;34 Suppl 3:214–20.
16. Attin T. Methods for assessment of dental erosion. *Monogr oral Sci* 2006;20:152–72.
17. Field J, Waterhouse P, German M. Quantifying and qualifying surface changes on dental hard tissues in vitro. *J Dent* 2010;38 Suppl 3:182–90.
18. Karda B, Jindal R, Mahajan S, Sandhu S, Sharma S, Kaur R. To analyse the erosive potential of commercially available drinks on dental enamel and various tooth coloured restorative materials - An in-vitro study. *J Clin Diagnostic Res* 2016;10 Suppl 5:ZC117–21.
19. Grenby TH. Methods of assessing erosion and erosive potential. *Eur J Oral Sci*1996;104 Suppl 2:207–14.
20. Wan Bakar WZ, Abdullah A, Hussien A. Erosion effect of acidic drinks on two types of glass ionomer cement. *Malays Dent J* 2011;33 Suppl 2:27–32.
21. Aliping-Mckenzie M, Linden RWA, Nicholson JW. The effect of coca-cola and fruit juices on the surface hardness of glass-ionomers and “compomers”. *J Oral Rehabil* 2004;31 Suppl 11:1046–52.
22. Bakar WZW, McIntyre J. Susceptibility of selected tooth-coloured dental materials to damage by common erosive acids. *Aust Dent J* 2008;53 Suppl 3:226–34.
23. Xavier AM, Sunny SM, Rai K, Hegde AM. Repeated exposure of acidic beverages on esthetic restorative materials: An in-vitro surface microhardness study. *J Clin Exp Dent* 2016;8 Suppl 3:e312–7.
24. Musfirah S, Mustain B, Alkadhim AH, Fatah FA, Jaafar A. Effect of tropical fruit juices on surface roughness of tooth coloured restorative materials. *J Dent Sci Res Ther* 2017;1 Suppl 1:26–9.
25. Hamouda IM. Effects of various beverages on hardness, roughness, and solubility of esthetic restorative materials. *J Esthet Restor Dent* 2011;23 Suppl 5:315–22.
26. Perera D, Yu SCH, Zeng H, Meyers IA, Walsh LJ. Acid resistance of glass ionomer cement restorative materials. *J Bioeng* 2020;7 Suppl 4:150.
27. McComb D, Erickson RL, Maxymiw WG, Wood RE. A clinical comparison of glass ionomer , resin-modified glass ionomer and resin composite restorations in the treatment of cervical caries in xerostomic head and neck radiation patients. *Oper Dent* 2002;27 Suppl 5:430-7.
28. Viana ÍEL, Alania Y, Feitosa S, Borges AB, Braga RR, Scaramucci T. Bioactive materials subjected to erosion/abrasion and their influence on dental tissues. *Oper Dent* 2020;45 Suppl 3:E114–23.

29. Chibinski AC. In vitro evaluation of the impact of erosive/abrasive challenge in glass ionomer cements. *Biomed J Sci &Tech Res* 2017;1 Suppl 5:1263–6.
30. Zaluzniak I, Palamara JEA, Wong RHK, Cochrane NJ, Burrow MF, Reynolds EC. Ion release and physical properties of CPP-ACP modified GIC in acid solutions. *J Dent* 2013;41 Suppl 5:449–54.
31. L Zheng, J Zheng, Y F Zhang, L M Qian, Z R Zhou. Effect of CPP-ACP on the remineralization of acid-eroded human tooth enamel : nanomechanical properties and microtribological behaviour study. *J. Phys D* 2013;46:404006.
32. Scardini IL. Effect of CPP-ACP on enamel eroded extrinsically: in vitro study. *Rev Gauch Odontol* 2018;66 Suppl 1:21–8.
33. Brasil VLM, Carlo HL, Santos RL, Lima BASG. Protective effect of calcium nanophosphate and CPP-ACP agents on enamel erosion. *Braz Oral Res* 2013;27 Suppl 6:463-70.
34. Mahasweta Joshi, Nikhil Joshi, Rahul Kathariya, Prabhakar Angadi, Sonal Raikar. Techniques to Evaluate Dental Erosion: A Systematic Review of Literature. *J Clin Diagn Res* 2016;10 Suppl 10:ZEO1–ZEO7.
35. Joshi N, Patil NP, Patil SB. The abrasive effect of a porcelain and a nickel-chromium alloy on the wear of human enamel and the influence of a carbonated beverage on the rate of wear. *J Prosthodont* 2010;19 Suppl 3:212–7.
36. Willershausen B, Schulz-Dobrick B GC. In vitro evaluation of enamel remineralisation by a casein phosphopeptide-amorphous calcium phosphate paste. *Oral Health Prev Dent* 2009;7 Suppl 1:13–21.
37. Hannig M, Balz M. Influence of in vivo formed salivary pellicle on enamel erosion. *Caries Res* 1999;33 Suppl 5:372–9.
38. Cheung A, Zid Z, Hunt D, McIntyre J. The potential for dental plaque to protect against erosion using an in vivo-in vitro model - A pilot study. *Aust Dent J* 2005;50 Suppl 4:228–34.
39. Gracia LH, Rees GD, Brown A, Fowler CE. An in vitro evaluation of a novel high fluoride daily mouthrinse using a combination of microindentation, 3D profilometry and DSIMS. *J Dent* 2010;38 Suppl 3:S12–20.
40. Hara AT, Zero DT. Analysis of the erosive potential of calcium-containing acidic beverages. *Eur J Oral Sci* 2008;116 Suppl 1:60–5.
41. White I, McIntyre J, Logan R. Studies on dental erosion: An in vitro model of root surface erosion. *Aust Dent J* 2001;46 Suppl 3:203–7.
42. Schlueter N, Hara A, Shellis RP, Ganss C. Methods for the measurement and characterization of erosion in enamel. *Caries Res* 2011;45 Suppl 1:13–23.
43. Maev RG, Denisova LA, Maeva EY, Denisov AA. New data on histology and physico-mechanical properties of human tooth tissue obtained with acoustic microscopy. *Ultrasound Med Biol* 2002;28 Suppl 1:131–6.
44. Ślak B, Ambroziak A, Strumban E, Maev RG. Enamel thickness measurement with a high frequency ultrasonic transducer-based hand-held probe for potential application in the dental veneer placing procedure. *Acta Bioeng Biomech* 2011;13 Suppl 1:65–70.
45. Barbour ME, Rees JS. The laboratory assessment of enamel erosion: A review. *J Dent* 2004;32 Suppl 8:591–602.
46. Fowler CE, Gracia L, Edwards MI, Rees GD, Brown A. Fluoride penetration from toothpastes into incipient enamel erosive lesions investigated using dynamic secondary ion mass spectrometry. *J Clin Dent* 2009;20 Suppl 6:186–91.
47. Vartanian LR, Schwartz MB, Brownell KD. Effects of soft drink consumption on nutrition and health: A systematic review and meta-analysis. *Am J Public Health* 2007;97 Suppl 4:667–75.
48. Al-Malik MI, Holt RD, Bedi R. Clinical and photographic assessment of erosion in 2-5-year-old children in Saudi Arabia. *Community Dent Health* 2001;18 Suppl 4:232–5.
49. Pretty IA, Edgar WM, Higham SM. The validation of quantitative light-induced fluorescence to quantify acid erosion of human enamel. *Arch Oral Biol* 2004;49 Suppl 4:285–94.
50. Angmar-Månsson B, Ten Bosch JJ. Quantitative light-induced fluorescence (QLF): A method for assessment of incipient caries lesions. *Dentomaxillofacial Radiol* 2001;30 Suppl 6:298–307.
51. Ando M, Hall AF, Eckert GJ, Schemehorn BR, Analoui M, Stookey GK. Relative ability of laser fluorescence techniques to quantitate early mineral loss in vitro. *Caries Res* 1997;31 Suppl 2:125–31.
52. Grenby TH, Mistry M, Desai T. Potential dental effects of infants' fruit drinks studied in vitro. *Br J Nutr* 1990;64 Suppl 1:273–83.
53. Neves BG, Farah A, Lucas E, de Sousa VP, Maia LC. Are paediatric medicines risk factors for dental caries and dental erosion? *Community Dent Health* 2010;27 Suppl 1:46–51.
54. Hughes JA, Jandt KD, Baker N, Parker D, Newcombe RG, Eisenburger M, et al. Further modification to soft drinks to minimise erosion: A study in situ. *Caries Res* 2002;36 Suppl 1:70–4.
55. Louwse C, Kjaeldgaard M, Huysmans MCDNJM. The reproducibility of ultrasonic enamel thickness

- measurements: An in vitro study. *J Dent* 2004;32 Suppl 1:83–9.
56. Paiva L, Fidalgo TKS, Costa LP, Maia LC, Balan L, Anselme K, et al. Antibacterial properties and compressive strength of new one-step preparation silver nanoparticles in glass ionomer cements ( NanoAg-GIC ). *J Dent* 2018;69:102–9.
  57. Elsaka SE, Hamouda IM, Swain M V. Titanium dioxide nanoparticles addition to a conventional glass-ionomer restorative : Influence on physical and antibacterial properties. *J Dent* 2011;39 Suppl 9:589–98.
  58. Hench LL, Xynos ID, Polak JM, Hench LL, Xynos ID, Polak JM. Bioactive glasses for in situ tissue regeneration. *J Biomater Sci Polym Ed* 2004;15 Suppl 4:543-62.
  59. Yli-urpo H, Lassila L V J, Narhi Timo, Vallittu P K. Compressive strength and surface characterization of glass ionomer cements modified by particles of bioactive glass. *Dent Mater*2005;21Suppl 3:201-9.
  60. Lohbauer U, Frankenberger R, Clare A, Petschelt A, Greil P. Toughening of dental glass ionomer cements with reactive glass fibres. *Biomater*2004;25 Suppl 22:5217–25.
  61. Garoushi S, Vallittu P, Lassila L. Hollow glass fibers in reinforcing glass ionomer cements. *Dent Mater* 2017;33 Suppl 2:e86–e93.
  62. Alireza Moshaverinia, Sahar Ansari, Maryam Moshaverinia, Nima Roohpour, Jawwad A Darr, Ihtesham Rehman. Effects of incorporation of hydroxyapatite and fluoroapatite nanobioceramics into conventional glass ionomer cements ( GIC ). *Acta Biomater*2008;4 Suppl 2:432–40.
  63. Lee J, Lee Y, Choi B, Lee J, Choi H, Son H, et al. Physical properties of resin-reinforced glass ionomer cement modified with micro and nano-hydroxyapatite. *J Nanosci Nanotechnol* 2010;10 Suppl 8:5270-6.
  64. Moheet IA, Luddin N, Ab Rahman I, Masudi SM, Kannan TP, Abd Ghani NRN. Evaluation of mechanical properties and bond strength of nano-hydroxyapatite-silica added glass ionomer cement. *Ceram Int* 2018;44 Suppl 8:9899–906.
  65. Bertolini MJ, Palma-Dibb RG, Zaghete MA, Gimenes R. Evaluation of glass ionomer cements properties obtained from niobium silicate glasses prepared by chemical process. *J Non Cryst Solids* 2005;351 Suppl 6–7:466–71.
  66. Xie D, Feng D, Chung ID, Eberhardt AW. A hybrid zinc-calcium-silicate polyalkenoate bone cement. *Biomater* 2003;24 Suppl 16:2749–57.
  67. Rahman IA, Ghazali NAM, Bakar WZW, Masudi SM. Modification of glass ionomer cement by incorporating nanozirconia-hydroxyapatite-silica nano-powder composite by the one-pot technique for hardness and aesthetics improvement. *Ceram Int* 2017;43 Suppl 16:13247–53.
  68. Wan Bakar WZ. Novel upgrading of conventional glass ionomer cement using nanohydroxyapatite, silica and zirconia. *On J Dent & Oral Heal* 2020;3 Suppl 5:17–9.
  69. Al H, Palamara JEA, Messer HH, Burrow MF, Reynolds EC. The incorporation of casein phosphopeptide – amorphous calcium phosphate into a glass ionomer cement. *Dent Mater* 2011;27 Suppl 3:235–43.
  70. Oshiro M, Yamaguchi K, Takamizawa T, Inage H, Watanabe T, Irokawa A, et al. Effect of CPP-ACP paste on tooth mineralization : an FE-SEM study. *J Oral Sci* 2007;49 Suppl 2:115-20.
  71. Prabhadevi Maganur, V Satish, A R Prabhakar, Srinivas Namineni. Effect of soft drinks and fresh fruit juice on surface roughness of commonly used restorative materials. *Int J Clin Pediatr Dent*. 2015;8(1):1–5.
  72. Gray JA. Kinetics of enamel dissolution during formation of incipient caries-like lesions. *Arch Oral Biol* 1966;11 Suppl 4:397-22.
  73. Van der Horst G, Wesso I, Burger AP, Dietrich DL, Grobler SR. Chemical analysis of cooldrinks and pure fruit juices - some clinical implications. *S Afr Med J* 1984;66 Suppl 20:755–8.
  74. Nourmohammadi J, Salarian R, Solati-Hashjin M, Moztarzadeh F. Dissolution behavior and fluoride release from new glass composition used in glass ionomer cements. *Ceram Int* 2007;33 Suppl 4:557–61.

Table 1: Articles sources

Electronic databases	Number of articles
PubMed	30
Scopus	24
Web of Science	20
<b>Total</b>	<b>74</b>